

# A multicentre longitudinal study of flortaucipir ( $^{18}\text{F}$ ) in normal ageing, mild cognitive impairment and Alzheimer's disease dementia

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The advent of tau-targeted PET tracers such as flortaucipir ( $^{18}\text{F}$ ) (flortaucipir, also known as  $^{18}\text{F}$ -AV-1451 or  $^{18}\text{F}$ -T807) have made it possible to investigate the sequence of development of tau in relationship to age, amyloid- $\beta$ , and to the development of cognitive impairment due to Alzheimer's disease. Here we report a multicentre longitudinal evaluation of the relationships between baseline tau, tau change and cognitive change, using flortaucipir PET imaging. A total of 202 participants 50 years old or older, including 57 cognitively normal subjects, 97 clinically defined mild cognitive impairment and 48 possible or probable Alzheimer's disease dementia patients, received flortaucipir PET scans of 20 min in duration beginning 80 min after intravenous administration of 370 MBq flortaucipir ( $^{18}\text{F}$ ). On separate days, subjects also received florbetapir amyloid PET imaging, and underwent a neuropsychological test battery. Follow-up flortaucipir scans and neuropsychological battery assessments were also performed at 9 and 18 months. Fifty-five amyloid- $\beta$ + and 90 amyloid- $\beta$ - subjects completed the baseline and 18-month study visits and had valid quantifiable flortaucipir scans at both time points. There was a statistically significant increase in the global estimate of cortical tau burden as measured by standardized uptake value ratio (SUVr) from baseline to 18 months in amyloid- $\beta$ + but not amyloid- $\beta$ - subjects (least squared mean change in flortaucipir SUVr :  $0.0524 \pm 0.0085$ ,  $P < 0.0001$  and  $0.0007 \pm 0.0024$   $P = 0.7850$ , respectively), and a significant association between magnitude of SUVr increase and baseline tau burden. Voxel-wise evaluations further suggested that the regional pattern of change in flortaucipir PET SUVr over the 18-month study period (i.e. which regions exhibited the greatest change) also varied as a function of baseline global estimate of tau burden. In subjects with lower global SUVr, temporal lobe regions showed the greatest flortaucipir retention, whereas in subjects with higher baseline SUVr, parietal and frontal regions were increasingly affected. Finally, baseline flortaucipir and change in flortaucipir SUVr were both significantly ( $P < 0.0001$ ) associated with changes in cognitive performance. Taken together, these results provide a preliminary characterization of the longitudinal spread of tau in Alzheimer's disease and suggest that the amount and location of tau may have implications both for the spread of tau and the cognitive deterioration that may occur over an 18-month period.

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**Abbreviations:** MCI = mild cognitive impairment; MMSE = Mini-Mental State Examination; MUBADA = multi-block barycentric discriminant analysis; NFT = neurofibrillary tangle; SUVr = standardized uptake value ratio

## Introduction

Alzheimer's disease is characterized pathologically by extracellular accumulation of aggregated amyloid- $\beta$  fragments, typically associated with degenerating neurites (amyloid- $\beta$  neuritic plaques) and by intracellular aggregates of abnormally phosphorylated microtubule-associated tau protein (neurofibrillary tangles, NFTs). Although the density of both amyloid- $\beta$  neuritic plaques and NFTs at autopsy has been shown to be correlated with ante-mortem cognitive impairment, the degree of association with cognitive impairment has been reported to be greater for NFTs than for neuritic plaques (Cummings *et al.*, 1996; Berg *et al.*, 1998; Nelson *et al.*, 2007, 2012). Moderate-to-frequent neocortical amyloid- $\beta$  neuritic plaques, consistent with a high level of Alzheimer's disease pathology (Hyman *et al.*, 2012), may be present in 30–50% of clinically normal individuals (Hulette *et al.*, 1998; Price and Morris, 1999; Bennett *et al.*, 2005; Nelson *et al.*, 2007), whereas tau pathology in clinically normal individuals is limited to NFTs in the mesial temporal lobe (entorhinal cortex, adjacent hippocampus, amygdala), and to a lesser extent, inferior temporal regions (Bouras *et al.*, 1994; Price and Morris, 1999; Knopman *et al.*, 2003; Bennett *et al.*, 2005). Widespread neocortical tau deposition, consistent with high Alzheimer's disease tangle pathology, is associated with both significant cognitive impairment and the presence of moderate-to-frequent amyloid- $\beta$  neuritic plaques (Tomlinson *et al.*, 1970; Knopman *et al.*, 2003; Bennett *et al.*, 2005; Nelson *et al.*, 2007, 2009, 2012). These findings have led to speculation that development of amyloid and tau pathology may begin independently (Nelson *et al.*, 2009; Mungas *et al.*, 2014) but that amyloid- $\beta$  neuritic plaques may potentiate the spread of NFTs, the more proximal cause of neuronal damage and cognitive impairment in Alzheimer's disease (Nelson *et al.*, 2007).

The advent of PET imaging agents targeting amyloid- $\beta$  and tau has enabled further exploration of these relationships in living subjects. Three ligands, florbetapir ( $^{18}\text{F}$ ), florbetaben ( $^{18}\text{F}$ ) and flutemetamol ( $^{18}\text{F}$ ) are now approved in major international regions for use in PET imaging of amyloid- $\beta$  neuritic plaques (Clark *et al.*, 2012; Curtis *et al.*, 2015; Sabri *et al.*, 2015). Subjects clinically diagnosed with Alzheimer's disease dementia or mild cognitive impairment (MCI) likely due to Alzheimer's disease have been shown to have worse cognitive performance (Pike *et al.*, 2007; Johnson *et al.*, 2013), and to deteriorate more rapidly

(Doraiswamy *et al.*, 2014; Ma *et al.*, 2014; Baker *et al.*, 2017), if amyloid-positive (amyloid- $\beta$ +) than if amyloid-negative (amyloid- $\beta$ -) by PET scan.

More recently, several new tracers targeted at tau NFTs have been reported (Maruyama *et al.*, 2013; Xia *et al.*, 2013; Chien *et al.*, 2014; Okamura *et al.*, 2014; Harada *et al.*, 2016; Hostetler *et al.*, 2016; Declercq *et al.*, 2017; Saint-Aubert *et al.*, 2017; Villemagne *et al.*, 2017; Betthausen *et al.*, 2019; Wong *et al.*, 2018). Although the scope of investigation is still limited for many of these agents, some general themes have begun to emerge, particularly for the most widely distributed of the tau targeted PET tracers, flortaucipir ( $^{18}\text{F}$ ) (flortaucipir,  $^{18}\text{F}$ -AV-1451; T807). The pattern of flortaucipir retention on PET imaging parallels the pattern of NFT accumulation reported in autopsy series (Braak *et al.*, 2006; Schwarz *et al.*, 2016). In clinically normal subjects with a negative amyloid PET scan, flortaucipir retention is limited largely to medial temporal lobe. In subjects with positive amyloid PET scans, cross-sectional comparisons suggest increasing and progressive flortaucipir retention in lateral temporal lobe, posterior association cortices and, finally, frontal cortex. This corresponds with increases in estimates of overall tau burden (e.g. cortical composite standardized uptake value ratios, SUVr) across clinical disease stages from clinically normal to MCI to Alzheimer's disease dementia (Brier *et al.*, 2016; Cho *et al.*, 2016a; Johnson *et al.*, 2016; Lockhart *et al.*, 2016; Schwarz *et al.*, 2016; Schöll *et al.*, 2016; Pontecorvo *et al.*, 2017b). The cortical composite tau PET SUVr also appears to be correlated with cortical amyloid burden (Pontecorvo *et al.*, 2017b). But, the regional distribution of the tau tracer PET signal differs from that of amyloid PET tracers, particularly at early disease stages (Brier *et al.*, 2016; Cho *et al.*, 2016a, b; Harada, 2016; Schöll *et al.*, 2016; Pontecorvo *et al.*, 2017b). Cortical composite tau PET SUVr has also been reported to correlate with degree of cognitive impairment (Okamura *et al.*, 2014; Cho *et al.*, 2016b; Johnson *et al.*, 2016; Pontecorvo *et al.*, 2017b), but the strength of this relationship has varied across studies.

Despite the growing cross-sectional tau PET imaging literature, only one study to date has examined longitudinal change in flortaucipir PET signal (Jack *et al.*, 2018). This study included 59 amyloid- $\beta$ - cognitively unimpaired, 37 amyloid- $\beta$ + cognitively unimpaired and 30 amyloid- $\beta$ + cognitively impaired subjects who underwent flortaucipir PET at baseline and 12–15 months. Amyloid- $\beta$ + impaired

subjects showed increases ( $\sim 3\%$  per year) in flortaucipir PET signal (SUVr) across most brain regions, whereas amyloid- $\beta$ - unimpaired patients showed little change. Amyloid- $\beta$ + unimpaired subjects also showed low accumulation of PET signal in most brain regions but significantly more accumulation ( $\sim 0.5\%$  per year) than amyloid- $\beta$ - subjects in temporal regions and posterior cingulate.

Further evaluation of the way in which tau accumulation, as assessed by PET imaging, changes over time could be critical to understanding the interaction of amyloid and tau in promoting neurodegeneration and cognitive impairment in Alzheimer's disease (Jack *et al.*, 2016). The present study was therefore designed to provide an exploratory evaluation of the changes in flortaucipir PET tau signal in clinically defined cognitively normal, MCI and Alzheimer's disease dementia subjects, and the association between tau PET signal and 18 month cognitive change in amyloid- $\beta$ + subjects, over an 18 month period. Recently, we have reported the cross-sectional baseline PET and cognitive data from this study (Pontecorvo *et al.*, 2017b). We now report on the longitudinal change in tau PET imaging and the association of flortaucipir PET and longitudinal cognitive performance.

## Materials and methods

### Study participants

As described previously (Pontecorvo *et al.*, 2017b), 223 subjects were recruited at 25 sites (NCT# 02016560). Sixteen of these subjects were enrolled as a young control group ( $< 50$  years of age) with baseline, but not longitudinal, flortaucipir scans. An additional five enrolled subjects were excluded from the present longitudinal analysis—three because their baseline scans were unusable due to technical failure, one because no florbetapir scan was available, and one because no baseline flortaucipir scan was obtained. Thus, a total of 202 subjects (57 clinically defined cognitively normal, 97 MCI subjects, and 48 subjects with clinically-defined possible or probable Alzheimer's disease) were at least 50 years of age, had baseline scans that were quantifiable using the target and reference regions described below, and were eligible for longitudinal analysis. Of these, 33 subjects discontinued before 9 months and an additional 21 discontinued between 9 and 18 months. One subject was excluded from the 9-month analysis (but not 18 months) and three subjects were excluded from the 18-month analysis due to scan technical issues. Thus, 168 subjects completed the 9-month visit and 145 subjects completed the 18-month visit with valid scan and cognitive data (Supplementary Fig. 2 and Supplementary Table 5).

### Diagnostic criteria

Subjects were classified as cognitively normal if they had no evidence of cognitive impairment by history or examination and had a screening visit Mini-Mental State Examination (MMSE)  $> 29$ . MCI subjects had a diagnosis consistent with National Institute of Aging (NIA)-Alzheimer's Association

clinical criteria (MCI-Alzheimer's disease; Albert *et al.*, 2011), were  $\geq 50$  years of age and had an MMSE  $> 24$ . Subjects in the clinically diagnosed Alzheimer's disease/Alzheimer's disease dementia group were  $\geq 50$  years of age, met NIA-Alzheimer's Association core clinical criteria for possible or probable Alzheimer's disease (McKhann *et al.*, 2011) and had an MMSE  $> 10$ . Subjects were excluded from participation if they were females of childbearing potential not using adequate contraception, had a history of stroke, current clinically significant cerebrovascular disease, drug or alcohol abuse or dependence, or if they were participating in a trial with other experimental drugs.

### Ethics committee

This protocol was approved by the relevant institutional review boards and all subjects or authorized representatives signed informed consent prior to conduct of study procedures. This trial was conducted in compliance with the Declaration of Helsinki and the International Conference on Harmonization guideline on good clinical practice (World Medical Association, 1997).

### Study assessments

At baseline, all subjects underwent a clinical diagnostic interview, and a cognitive/functional test battery including MMSE, Alzheimer's Disease Assessment Scale 11-item cognitive subscale (ADAS-Cog<sub>11</sub>), and the Pfeffer Functional Activities Questionnaire (FAQ). An MRI scan performed at screening or within 6 months prior to enrolment ruled out significant CNS lesions and included a 3D T<sub>1</sub>-weighted sequence that was used for processing the PET images. Additionally, all subjects underwent a florbetapir amyloid PET scan. Flortaucipir PET scans, MRI, and cognitive assessments were repeated at the follow-up visits at  $9 \pm 2$  and  $18 \pm 2$  months. Vital signs, laboratory values and ECG were obtained prior to and after each flortaucipir PET scan, and adverse events were monitored for 48 h post-scan.

### Imaging acquisition and analysis

For flortaucipir PET imaging, subjects received an intravenous infusion of  $\sim 370$  MBq (10 mCi) of flortaucipir ( $^{18}\text{F}$ ), followed  $\sim 80$  min post-dose by a continuous 20-min brain scan, acquired as four 5-min frames. For florbetapir PET imaging, subjects received an intravenous infusion of  $\sim 370$  MBq (10 mCi) florbetapir ( $^{18}\text{F}$ ), followed 50 min later by a 10-min brain PET scan acquired as two 5-min frames. All PET data were reconstructed using scanner-specific protocols with the following parameter selections: iterative reconstruction algorithm (FORE, OSEM or RAMLA), 3–6 iterations, 16–33 subsets,  $2.0$ – $2.67$  mm  $\times$   $2.0$ – $2.67$  mm  $\times$   $2.0$ – $4.25$  mm voxel size. Post-reconstruction Gaussian filters of 3–5 mm were applied (except for Philips scanners where the 'Normal' or 'Sharp' relaxation parameter setting was used). Detector response modelling was not used. Time of flight reconstruction was used at one site.

Florbetapir PET images were visually interpreted as either amyloid- $\beta$ + or amyloid- $\beta$ - by two experienced readers (A.K.A. and M.D.D.) with access to quantitative information (VisQ read, Pontecorvo *et al.*, 2017a).

For the analysis of flortaucipir PET data, the 5-min PET images were motion corrected, as well as corrected for time of acquisition to be equivalent to an 80 min post-injection acquisition time (see below), then summed into a single image. The summed image was then co-registered to the subject's T<sub>1</sub>-weighted MRI image. The 9- and 18-month PET images were similarly motion and time corrected and summed, then aligned first to the baseline PET image and then to the corresponding MRI image using the same co-registration parameters as the baseline PET scan. The unified segmentation and normalization algorithm in SPM8 was used to transform the T<sub>1</sub> MRI images to MNI atlas space while simultaneously segmenting them into probabilistic tissue maps corresponding to grey matter, white matter, and CSF. The MRI-to-atlas transformation matrix was then used for spatial normalization of the co-registered flortaucipir PET data (Fonov *et al.*, 2011).

Previous studies (Shcherbinin *et al.*, 2016) have suggested that flortaucipir SUVR values may not reach a stable plateau, but may continue to increase throughout the potential imaging window (i.e. up to 150 min post-injection). Consequently, differences in the delay from injection to scan acquisition times across the baseline, 9- and 18-month scans could result in systematic differences in SUVR, with longer delay times leading to higher SUVR, particularly in patients with higher tau burden. Correction factors to address this concern are determined as follows: for a dynamic PET image with  $n$  time frames, acquisition time correction factors are calculated for each 3D image voxel as the slope  $m$  of the linear regression line through  $n$  time points, multiplied by the time offset between the desired acquisition time window and the actual acquisition time window. Thus, for each voxel a corrected average value could be calculated as:

$$y_{\text{CORR}} = y_{\text{AVG}} + m(t_{\text{mid\_desired}} - t_{\text{mid\_acquired}}) \quad (1)$$

where  $t_{\text{mid\_desired}}$  is the midpoint of the desired acquisition time window,  $t_{\text{mid\_acquired}}$  is the midpoint of the actual acquisition time window,  $y_{\text{AVG}}$  is the uncorrected mean voxel value and  $y_{\text{CORR}}$  is the time-corrected mean voxel value.

This generates an 'image' of  $y_{\text{CORR}}$  values which replace the original mean 20-min image and can be divided by the calculated PERSI value to produce an SUVR image (Southehal *et al.*, 2018).

Global cortical flortaucipir retention was summarized for each patient by an SUVR. The target volumes of interest (SUVR numerator) consisted of a weighted average of voxels found, through multi-block barycentric discriminant analysis (MUBADA), to contribute to discrimination between amyloid- $\beta$ + clinically defined MCI and Alzheimer's disease dementia and amyloid- $\beta$ - cases at baseline. Although voxels from all brain lobes are included in this target region, the volume of interest is weighted more heavily toward voxels in posterior and lateral temporal lobe, parietal lobe and association regions of occipital cortex and exhibits higher weights in the left hemisphere (Devous *et al.*, 2018). The reference region (SUVR denominator) was parametrically derived by extracting a voxel intensity-histogram from an atlas-based white matter region, then fitting a bimodal Gaussian distribution to the histogram and using the full-width at half-maximum (FWHM) range of voxels in the lower intensity peak to construct a reference region map (PERSI reference region, Southehal *et al.*, 2018). The result is the MUBADA/PERSI flortaucipir SUVR for each

subject. For supplementary analyses, SUVR were also calculated for AAL regions and a composite as previously described (Pontecorvo *et al.*, 2017b). Test-retest variability for various flortaucipir SUVR calculation methods has previously been examined and has been reported to be  $\sim 0.0029 \pm 0.0288$  SUVR for the MUBADA/PERSI SUVR (Devous *et al.*, 2018).

Cortical surface maps were also created for each subject for the baseline, 9- and 18-month images. The baseline T<sub>1</sub>-weighted MRI volumes were run through FreeSurfer's version 5.3 cortical reconstruction program to generate subject-specific subcortical segmentations and delineate the pial and white matter surfaces (Fischl *et al.*, 2012). The cortical reconstructions were inspected visually for failed segmentations and/or surface errors. The motion- and time-corrected baseline, 9- and 18-month flortaucipir PET scans were registered to the bias-corrected T<sub>1</sub> MRI generated by FreeSurfer using FSL's FLIRT function with six degrees of freedom. The flortaucipir uptake halfway between the white and pial surfaces was then projected onto FreeSurfer's fsaverage template surface and smoothed by a white surface Gaussian filter with an FWHM of 5 mm. The smoothed surface maps were then normalized by each subject's PERSI reference value. Average maps were created across all amyloid- $\beta$ + subjects at baseline and 18 months and a subtraction image was used to illustrate average change in tau over 18 months. Additionally, amyloid- $\beta$ + subjects were stratified into four 'quartiles' based on their baseline MUBADA/PERSI flortaucipir SUVR values to further explore the voxel-wise change as a function of baseline flortaucipir PET signal.

All image processing and interpretation was performed blind to subject clinical status.

## Statistical methods

Demographic and baseline characteristics were summarized with descriptive statistics [mean, standard deviation (SD), for continuous variables; frequency and percentages for categorical information], across all subjects, by amyloid status (florbetapir PET amyloid- $\beta$ + / amyloid- $\beta$ -) and by diagnosis group. Two-way ANOVA tests were performed to evaluate differences between continuous variables across amyloid status and diagnosis groups, and Mantel-Hansel  $\chi^2$  tests were applied to evaluate difference of categorical variables across amyloid status and diagnosis groups.

To evaluate the tau change at 18 months, mixed models with repeated measures (MMRM) were fitted to assess change in MUBADA SUVR while controlling for baseline MUBADA SUVR and age in amyloid- $\beta$ + and amyloid- $\beta$ - groups separately, due to the concern of unequal variance in MUBADA SUVR changes observed between the amyloid- $\beta$ + and amyloid- $\beta$ - groups. Similar supplementary analyses were performed using the AAL composite/cerebellum SUVR values rather than MUBADA SUVR values.

To further explore the potential factors that affect tau accumulation, a multivariate regression model with stepwise selection technique was applied. The entry and elimination criteria were set at  $P = 0.20$  level due to the exploratory nature of this analysis, and the concern with this relatively small sample size. The model was run with amyloid- $\beta$ + impaired subjects (demented and MCI) only, using MUBADA SUVR change as the dependent variable. The predictors included in this model for assessment were as follows: baseline MUBADA SUVR,

florbetapir SUV<sub>r</sub>, MMSE, sex and baseline age. Similar supplementary analyses were performed using the AAL composite/cerebellum SUV<sub>r</sub> values rather than MUBADA SUV<sub>r</sub> values.

The relationship between cognitive assessments and tau level was assessed first with a simple correlation analysis. Baseline MUBADA SUV<sub>r</sub> versus MMSE change at 18 months, and change in MUBADA SUV<sub>r</sub> at 18 months versus MMSE change at 18 months were also visually displayed by scatter plots, in addition to the Pearson correlation analyses. A multivariate regression analysis with stepwise selection technique was applied to explore the contribution of each potential factor for cognitive deterioration, using amyloid-β+ impaired subjects. For this multivariate regression model, MMSE change at 18 months was used as a dependent variable, with predictors including baseline cognitive test score (i.e. MMSE), age, baseline American National Adult Reading Test (ANART; a surrogate for cognitive reserve/premorbid IQ), baseline florbetapir SUV<sub>r</sub>, APOE4 carrier status, baseline flortaucipir SUV<sub>r</sub> and/or change in flortaucipir SUV<sub>r</sub>. Entry and elimination criteria for including a predictor in the final model were set at  $P = 0.20$  level. Similar analyses were also performed with ADAS and FAQ as dependent variables. Similar supplementary analyses were performed using the AAL composite/cerebellum SUV<sub>r</sub> values rather than MUBADA SUV<sub>r</sub> values.

All analyses were conducted using SAS windows version 9.4. Because of the exploratory nature of this analysis, no adjustments were made for multiplicity.

## Data availability

Data that support the findings of this study are available from the corresponding author upon reasonable request.

## Results

### Study population baseline demographics and disposition

Table 1 shows the baseline characteristics of the 202 subjects eligible for longitudinal analysis. Supplementary Table 1 shows that the demographics for the 168 that completed the 9-month follow-up visit and the 145 that completed the 18-month visit with valid PET and cognitive data were similar to those for the baseline population. Mean age (years) increased by disease category (cognitively normal = 68.5; MCI = 70.8; clinically diagnosed Alzheimer's disease dementia = 73.9), in part because enrolment in the cognitively normal group was stratified by age to evenly cover a range from 50 to 80+ years of age. Amyloid-β+ subjects also tended to be older and more likely to be ApoE4 carriers than amyloid-β- subjects regardless of diagnostic category. The mean (SD) MMSE scores in the healthy control group were 29.5 (0.50) compared to 27.8 (1.78) in the MCI group and 21.9 (3.86) in the Alzheimer's disease dementia group. A total of 79 subjects that were classified as MCI or Alzheimer's disease

**Table 1** Demographics for all patients receiving flortaucipir PET

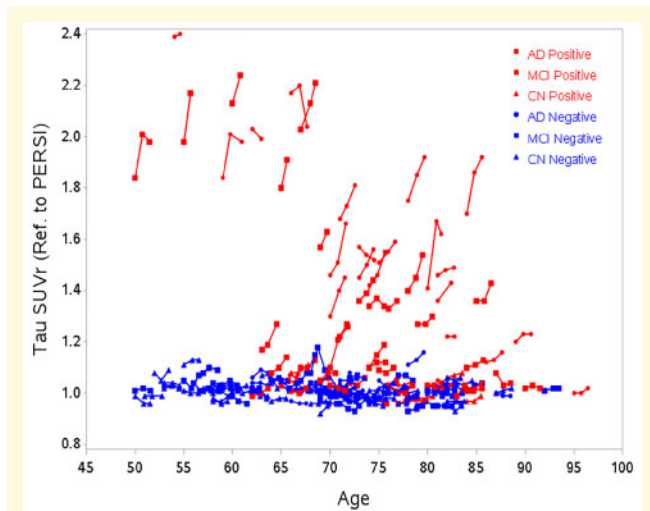
	Baseline population		
	Total	Amyloid-β+	Amyloid-β-
<i>n</i>	202	84	118
<b>Cognitively normal</b>			
<i>n</i>	57	5	52
Age, mean years (SD)	68.5 (10.38)	77.8 (7.01)	67.6 (10.25)
Gender: female, <i>n</i> (%)	26 (45.6)	2 (40.0)	24 (46.2)
Race: Caucasian, <i>n</i> (%)	46 (80.7)	5 (100)	41 (78.8)
Education, years (SD)	15.7 (1.94)	15.2 (2.28)	15.7 (1.92)
% APOE 4 carriers, <i>n</i> (%)	12 (21.1)	2 (40)	10 (19.2)
MMSE mean (SD)	29.5 (0.5)	29.6 (0.55)	29.5 (0.5)
<b>MCI</b>			
<i>n</i>	97	47	50
Age, mean years (SD)	70.8 (9.35)	72.7 (9.14)	69.1 (9.29)
Gender: female, <i>n</i> (%)	48 (49.5)	21 (44.7)	27 (54.0)
Race: Caucasian, <i>n</i> (%)	88 (90.7)	45 (95.7)	43 (86.0)
Education, years (SD)	15.8 (2.95)	16.1 (2.7)	15.5 (3.17)
% APOE 4 carriers, <i>n</i> (%)	46 (47.4)	28 (59.6)	18 (36)
MMSE mean (SD)	27.8 (1.78)	27.4 (1.83)	28.2 (1.66)
<b>Alzheimer's disease</b>			
<i>n</i>	48	32	16
Age, mean years (SD)	73.9 (9.17)	74.8 (10.1)	72.2 (6.93)
Gender: female, <i>n</i> (%)	28 (58.3)	21 (65.6)	7 (43.8)
Race: Caucasian, <i>n</i> (%)	45 (93.8)	31 (96.9)	14 (87.5)
Education, years (SD)	15.2 (2.43)	15 (2.78)	15.6 (1.5)
% APOE 4 carriers, <i>n</i> (%)	26 (54.2)	22 (68.8)	4 (25)
MMSE, mean (SD)	21.9 (3.86)	21.5 (4.1)	22.9 (3.24)

dementia were amyloid-β+ and 66 subjects were amyloid-β-; in the cognitively normal group five subjects were amyloid-β+ and 52 were amyloid-β-. Dementia/MCI subjects tended to prematurely dropout of the study at a higher rate than control subjects (51/145, 35% versus 4/57, 7%,  $P < 0.0001$ ) but there was no significant difference in the dropout rate between amyloid-β+ and amyloid-β- subjects (28/84, 33% and 28/119, 23%, respectively,  $P = 0.1000$ ).

### Change in flortaucipir SUV<sub>r</sub>

Figure 1 shows the flortaucipir SUV<sub>r</sub> values at the three study time points (baseline, 9 and 18 months) for individual subjects as a function of their age, diagnosis and amyloid status. Consistent with our previous analysis using an AAL-derived cortical composite target area and a cerebellar crus reference region (Pontecorvo *et al.*, 2017b), Table 2 shows that the baseline flortaucipir SUV<sub>r</sub> [mean (standard error, SE)] was significantly higher in the amyloid-β+ subjects compared to amyloid-β- subjects [1.3267 (0.0408) versus 1.0095 (0.0034), between-group difference  $P < 0.0001$ ]. In the amyloid-β+ group the flortaucipir SUV<sub>r</sub> [least squares mean (SE)] increased significantly from baseline to the 9- and 18-month visits [amyloid-β+ :

9-month = 0.0316 (0.0060), 18-month = 0.0524 (0.0085); both  $P < 0.0001$ ]. In the amyloid- $\beta^-$  group the flortaucipir SUVr was relatively unchanged with a least squares mean change in flortaucipir SUVr of  $-0.0003$  (0.0020) and 0.0007 (0.0024) at the 9- and 18-month follow-up visits, respectively ( $P > 0.78$ ). As has been reported previously (Pontecorvo *et al.*, 2017b), Fig. 1 also shows that, for the amyloid- $\beta^+$  group, baseline SUVr was inversely related to age ( $r = -0.57$ ,  $P \leq 0.0001$ ). Figure 2A shows that there was a significant relationship between baseline flortaucipir SUVr and change in SUVr across all subjects and within the amyloid- $\beta^+$  subjects only. There was also a trend in amyloid- $\beta^+$  subjects toward an inverse relationship between SUVr increase and age (Fig. 2B). However, when age, sex, baseline MUBADA SUVr and florbetapir SUVr were entered as covariates, only baseline flortaucipir SUVr emerged as a significant predictor of change from baseline



**Figure 1** Flortaucipir PET MUBADA/PERSI SUVr at baseline, 9 and 18 months for individual subjects. Each subject is plotted by age at baseline and follow-up time points on the x-axis. Symbols reflect clinical diagnosis [cognitively normal (CN), MCI, Alzheimer's disease (AD)]. Subjects shown in red were amyloid- $\beta^+$  and subjects in blue amyloid- $\beta^-$  by florbetapir amyloid PET scan. For amyloid- $\beta^+$  subjects baseline SUVr was inversely related to age ( $r = -0.57$ ,  $P \leq 0.0001$ ).

SUVr in the amyloid- $\beta^+$  subjects. (Table 3;  $P = 0.001$ ). Similar results (Supplementary Tables 2 and 3) were obtained using the previous (Pontecorvo *et al.*, 2017b) AAL composite target and cerebellar crus reference region.

## Surface map qualitative data: all patients

Figure 3 shows Freesurfer voxel-wise surface maps of mean flortaucipir SUVr values for amyloid- $\beta^+$  subjects at baseline, and the mean voxel-wise change from baseline to 18 months. Because the analysis above (Fig. 2A) suggested that baseline flortaucipir was a key determinant of SUVr change, we stratified amyloid- $\beta^+$  subjects into four 'quartiles' based on their baseline MUBADA SUVr values to explore possible differences in the average pattern of voxel-wise change with increasing baseline tau load. Figure 3 suggests that the group with the lowest flortaucipir SUVr at baseline (first quartile) showed little change in SUVr over 18 months. In the group with low flortaucipir SUVr (second quartile), 18-month increases in flortaucipir were seen predominantly in inferior and lateral temporal cortex and in posterior cingulate. In subjects with intermediate flortaucipir retention at baseline (third quartile) the areas of greatest average accumulation over 18 months included posterior lateral temporal cortex, lateral occipital cortex and medial and lateral parietal cortex. Finally, in subjects with the highest levels of flortaucipir SUVr at baseline (fourth quartile), areas of greatest accumulation over 18 months included medial parietal cortex and frontal cortex. Interestingly, areas such as lateral temporal and parietal cortex, which showed the greatest degree of change in the intermediate baseline flortaucipir SUVr group (third quartile), may have begun to plateau in the highest baseline SUVr group and did not show marked increases in signal over the 18-month study period. Surface maps showing  $P$ -values for voxel change from baseline yielded similar conclusions (Supplementary Fig. 3).

## Relationship to cognitive change

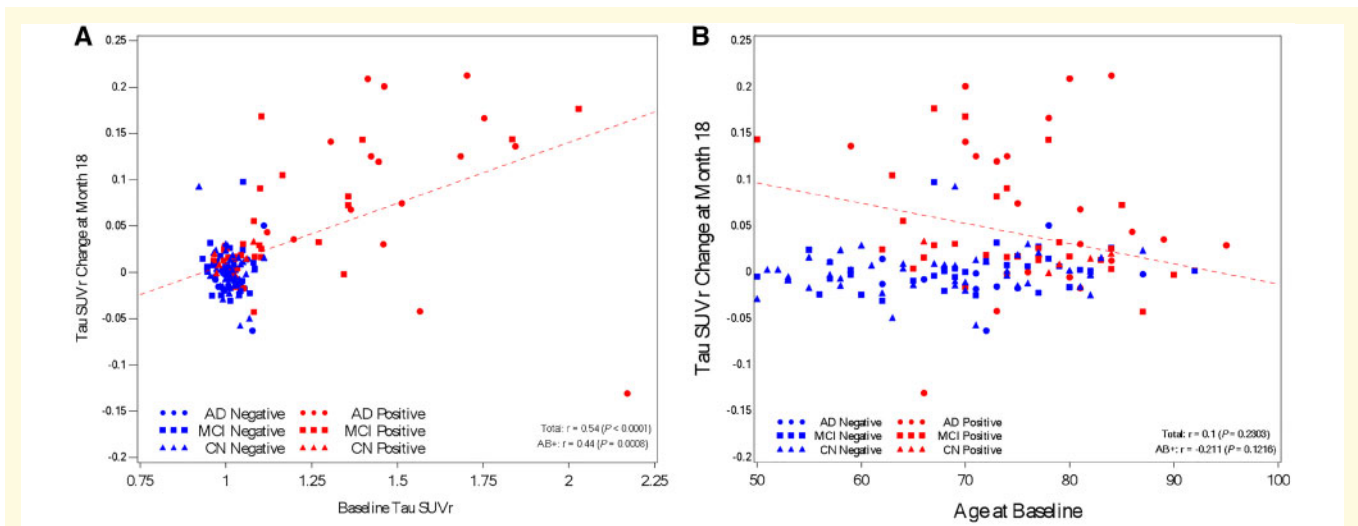
Figure 4A shows there was a moderate, but significant ( $P < 0.0001$ ), relationship between change in MUBADA SUVr and change in MMSE that was driven by the amyloid- $\beta^+$  subjects ( $r$  in amyloid- $\beta^+$  subjects =  $-0.55$ ). Figure

**Table 2** Change from baseline flortaucipir MUBADA SUVr

Amyloid- $\beta$ status	Baseline SUVr ( $\pm$ SE)	Visit	$n$	Mean change SUVr ( $\pm$ SE)	Mean % CFB SUVr	Least squares mean change SUVr ( $\pm$ SE)	$P$ -value
Amyloid- $\beta^-$	1.0095 (0.0034) <sup>a</sup>	9 months	102	$-0.0003$ (0.0019)	0	$-0.0003$ (0.0020)	0.8937
		18 months	90	0.0006 (0.0025)	0	0.0007 (0.0024)	0.7850
Amyloid- $\beta^+$	1.3267 (0.0408)	9 months	66	0.0339 (0.0070)	2.2	0.0316 (0.0060)	$< 0.0001$
		18 months	55	0.0526 (0.0095)	3.8	0.0524 (0.0085)	$< 0.0001$

CFB = change from baseline; SE = standard error.

<sup>a</sup>Different from amyloid- $\beta^+$ ,  $P < 0.0001$ .



**Figure 2** Correlation of baseline flortaucipir PET MUBADA SUVr (A) or age at baseline (B) with change from baseline flortaucipir PET MUBADA SUVr. Individual subjects are shown with symbols reflecting clinical diagnosis [cognitively normal (CN), MCI, Alzheimer’s disease (AD)]. Subjects shown in red were amyloid-β+ and subjects in blue amyloid-β– by florbetapir amyloid PET scan. Regression line is for amyloid-β+ subjects.

**Table 3** Multivariate regression model of MUBADA SUVr change at 18 months with stepwise selection technique

Fixed effect	Estimate ± SE	R-squared <sup>a</sup>	P-value <sup>b</sup>
Selected model			
Baseline MMSE	0.005 ± 0.0025	0.034	0.0691
Florbetapir SUVr	0.097 ± 0.0564	0.048	0.0931
Baseline MUBADA SUVr	0.117 ± 0.0334	0.174	0.0010
Overall R-squared		0.255	
Excluded effects			
Sex			0.5930
Age			0.8698

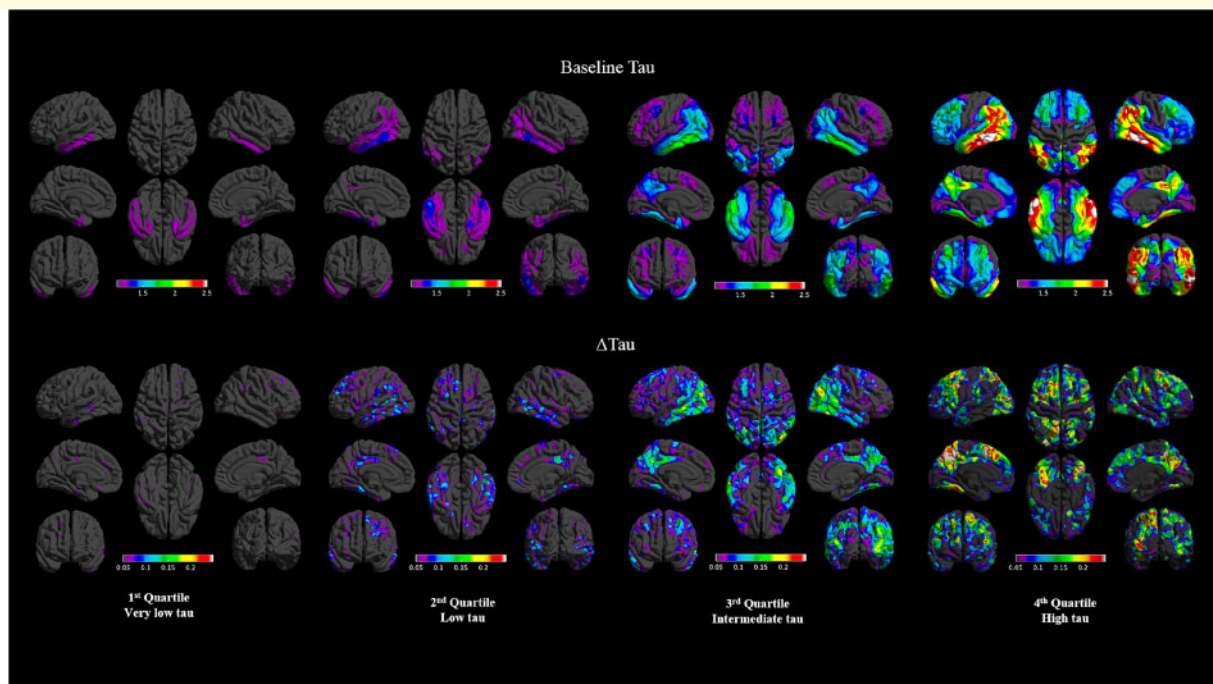
<sup>a</sup>Correlations for model effects are partial R-squared coefficients. Overall R-squared value is the result of the selected model.  
<sup>b</sup>P-values are results from an ANCOVA analysis adjusted for the reported covariates. SE = standard error.

4A suggests that although change in flortaucipir SUVr explains a relatively modest portion (~30%) of the variance in 18-month cognitive change, there may be a threshold effect, in that all but one of the amyloid-β+ subjects with at least a 0.06 unit SUVr change showed a decline in MMSE from baseline. Because analyses suggested a strong relationship between change in SUVr and baseline SUVr (Fig. 2A), the relationship between baseline SUVr and change in cognition was also evaluated. Figure 4B indicates there was also a correlation between baseline SUVr and MMSE change from baseline ( $r$  in amyloid-β+ subjects =  $-0.54$ ,  $P < 0.0001$ ). A multivariate regression analysis with stepwise selection method was attempted to evaluate the relative contribution of baseline versus change in flortaucipir SUVr to predict change in cognition

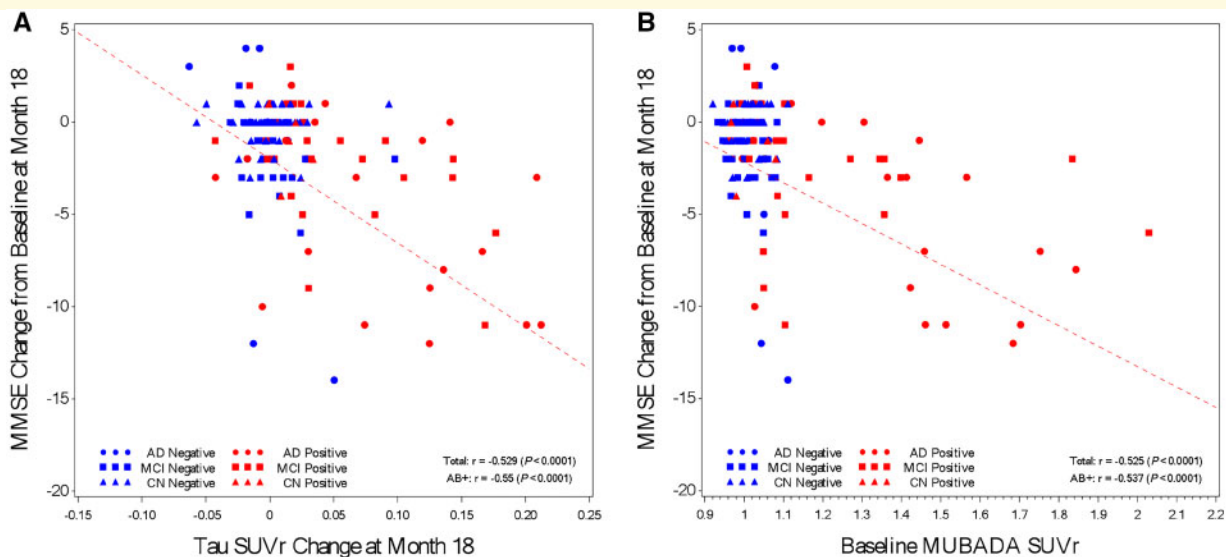
in amyloid-β+ subjects, in the context of other explanatory factors (e.g. age, APOE4 carrier status, baseline ANART, baseline florbetapir SUVr). However, sensitivity analyses indicated that the resultant model was unstable, possibly due to the limited sample size and the high degree of correlation between baseline SUVr and change in SUVr (~0.44 in amyloid-β+ subjects, 0.54 across all subjects); changes in value for just a few cases were sufficient to change the significance of baseline versus change in MUBADA SUVr as predictive factors. On the other hand, when change in SUVr was excluded from the model, baseline flortaucipir SUVr remained a significant predictor of all three measures of cognitive change (MMSE, ADAS, FAQ) even after correction for baseline test score, age, ANART and florbetapir SUVr (Table 4). Importantly, florbetapir SUVr did not survive for inclusion in any of the models when flortaucipir baseline SUVr was included. Similar results (Supplementary Table 4) were obtained using the previous (Pontecorvo *et al.*, 2017b) AAL composite target and cerebellar crus reference region.

## Discussion

In this multicentre longitudinal evaluation of tau change using flortaucipir PET imaging, we observed a statistically significant increase in the global estimate of cortical tau burden (flortaucipir SUVr) over 18 months. This increase was amyloid-dependent, correlated with baseline flortaucipir SUVr/tau burden, and was less pronounced in older compared to younger amyloid-positive subjects. Voxel-wise evaluations further suggested that the brain regions exhibiting the greatest changes in flortaucipir PET SUVr over the 18-month study period also varied as a function



**Figure 3** Freesurfer voxel-wise surface maps of mean flortaucipir SUVR values. For amyloid- $\beta$ + subjects at baseline (top), and the mean voxel-wise change from baseline to 18 months (bottom). Subjects were stratified into four 'quartiles' (columns) based on their baseline MUBADA SUVR values to better evaluate change in flortaucipir PET distribution as a function of baseline tau burden.



**Figure 4** Correlation of change from baseline flortaucipir PET MUBADA SUVR (A) or baseline flortaucipir PET MUBADA SUVR (B) with change from baseline MMSE. Individual subjects are shown with symbols reflecting clinical diagnosis [cognitively normal (CN), MCI, Alzheimer's disease (AD)]. Subjects shown in red were amyloid- $\beta$ + and subjects in blue amyloid- $\beta$ - by flortaucipir amyloid PET scan. Regression line is for amyloid- $\beta$ + subjects.

of baseline global estimate of tau burden. Finally, change in flortaucipir SUVR, and perhaps more importantly, baseline flortaucipir SUVR were significantly associated with changes in cognitive performance as assessed by MMSE, ADAS and FAQ.

The absence of a measurable change in flortaucipir SUVR in amyloid- $\beta$ - subjects (0.0005 SUVR units over 18 months), in contrast to the significant change in amyloid- $\beta$ + subjects, suggests that amyloid deposition may be a necessary antecedent for spread of tau beyond the temporal



**Table 4 Stepwise regression: predictors of cognitive change**

	Baseline MUBADA	Baseline Cog Test	Age	ANART	Florbetapir SUVr	APOE4	Model total
<b>MMSE</b>							
r <sup>2</sup>	0.301	NS	NS	0.050	NS	0.043	0.395
P	0.0016	> 0.2	> 0.2	0.058	> 0.2	0.0831	
<b>ADAS</b>							
r <sup>2</sup>	0.0667	NS	0.0328	0.2136	NS	NS	0.313
P	0.0210	> 0.2	0.1589	0.0087	> 0.2	> 0.2	
<b>FAQ</b>							
r <sup>2</sup>	0.13	NS	NS	NS	NS	NS	0.130
P	0.01	> 0.2	> 0.2	> 0.2	> 0.2	> 0.2	

ADAS = Alzheimer's Disease Assessment Scale 11-item cognitive subscale; FAQ = Pfeffer Functional Activities Questionnaire; NS = not significant.

lobe in Alzheimer's disease. It is worth noting that the amyloid-β<sup>-</sup> group in this study (in contrast to the recent study of Jack *et al.*, 2018) contained a significant number of cognitively impaired individuals (50 clinically diagnosed MCI, 16 possible/probable Alzheimer's disease dementia at baseline) so the pattern of cross-sectional and longitudinal change in flortaucipir PET signal observed in the amyloid-β<sup>+</sup> group cannot simply be attributed to the presence of impairment, but is likely associated with Alzheimer's disease pathology. Emerging evidence indicates that the sensitivity of flortaucipir and the regional pattern of flortaucipir retention may be different in non-Alzheimer's disease tauopathies than in Alzheimer's disease (Josephs *et al.*, 2016; McMillan *et al.*, 2016; Ossenkoppele *et al.*, 2016; Smith *et al.*, 2016; Hammes *et al.*, 2017; Marquié, 2017; Schonhaut *et al.*, 2017), and may even differ between Alzheimer's disease and associated dementias such as dementia with Lewy bodies (Gomperts *et al.*, 2016; Kantarci *et al.*, 2017). Thus, it remains to be determined whether the rates of longitudinal change observed in this study have any generalizability to non-Alzheimer's disease tauopathies.

Examination of individual changes in tau in Fig. 1, or the least squares mean change values at 9 and 18 months in Table 2, suggests that the change in global cortical tau is roughly linear for individual subjects over the 18-month period (e.g. the change over the first 9 months is comparable to change over the second 9 months). However, rate of change in tau accumulation might not be linear over the longer course of the disease. Figure 2 shows that the magnitude of change over the 18-month period varied as a function of the baseline SUVr value. Thus, it might be expected that over a longer period of time the rate of increase in the global estimate of tau might increase with disease severity. These results are consistent with the hypothesis of trans-synaptic spread of tau (De Calignon *et al.*, 2012; Liu *et al.*, 2012), in that it would be expected that the higher the baseline SUVr, the greater the number of neurons affected. This, in turn, would lead to a greater number of at risk synapses and thus, a greater degree of increase in tau over the observation period.

Voxel-wise analysis provided further evidence of a different rate and pattern of tau change as a function of flortaucipir global SUVr at baseline. In subjects with low or no elevation of flortaucipir retention at baseline, the greatest changes in SUVr were seen in inferior and lateral temporal cortex and in posterior cingulate. With increasing baseline tau burden, more posterior brain regions (e.g. occipital and parietal cortex) seemed to become important, whereas in subjects with the highest levels of flortaucipir SUVr at baseline, the areas of greatest accumulation also included frontal cortex. However, in subjects with the highest levels of flortaucipir SUVr at baseline, some regions such as lateral temporal and parietal cortex did not change substantially, suggesting that the tau pathology in these areas may have reached a plateau. This pattern of changes is consistent with cross-sectional descriptions of tau staging and provides preliminary longitudinal evidence that tau spread, at least at a group level, may follow the pattern predicted from cross-sectional autopsy studies. The results also provide some measure of caution regarding use of global measures of tau change as outcomes in longitudinal studies, since different regions may be changing at different rates over time depending on the severity and location of the initial/baseline tau burden.

A possible weakness of this study is that the proportion of amyloid-β<sup>-</sup> Alzheimer's disease dementia patients is higher (33%) than in some previous studies. This may be due in part to the use of a possible, rather than a probable Alzheimer's disease diagnosis as an entry criterion in the present study. For example, a 22% amyloid-β<sup>-</sup> rate was reported in a therapeutic trial of probable Alzheimer's disease subjects (Siemers *et al.*, 2016) whereas a recent study in patients seeking diagnosis reported that ~30% of subjects with possible Alzheimer's disease as a working diagnosis prior to scan were amyloid-β<sup>-</sup> by flortaucipir read (Pontecorvo *et al.*, 2017c). Although the amyloid-β<sup>-</sup> subjects reduce the power to examine changes in the population of interest (amyloid-β<sup>+</sup>/Alzheimer's disease pathology subjects), the amyloid-β<sup>-</sup> cohort does, as noted above, provide an interesting population to compare tau changes (or lack of changes) in the absence of amyloid. A potentially

more important weakness is the low number of amyloid- $\beta$ + clinically normal subjects in this study. This makes it difficult to evaluate tau/flortaucipir retention at the earliest stages of the Alzheimer's continuum.

Another weakness of this study is that the effects of age and baseline SUVr in this study were largely confounded. The younger subjects tended to have the highest baseline SUVr, and young age was also associated with increased change in SUVr from baseline to 18 months. The elevated baseline SUVr and more rapid increase in SUVr in the younger subjects over the 18-month study period may indicate a more aggressive Alzheimer's disease pathology in patients with younger age at onset. However, this finding may also reflect a survivor effect in the older subjects. Moreover, factors other than Alzheimer's disease pathology are increasingly likely to contribute to cognitive impairment as individuals age (Jack *et al.*, 2016). As a result of the additive effects of other neuropathology plus tau burden/Alzheimer's disease pathology, older subjects may have greater impairment than young subjects at any given level of pathology, and older subjects with the highest levels of tau burden/Alzheimer's disease pathology, comparable to that seen in the young subjects, might be too impaired to participate in a study of this type. The complicated relationship between age, tau burden and cognitive impairment has previously been reported both in tau PET studies (Cho *et al.*, 2017; Pontecorvo *et al.*, 2017b; Schöll *et al.*, 2017) and clinicopathological studies (Prohovnik *et al.*, 2006; Middleton *et al.*, 2011).

Overall the results of this study are similar in many respects to the longitudinal changes in tau accumulation recently reported by Jack *et al.* (2018). In both studies, amyloid- $\beta$ + cognitively impaired subjects showed longitudinal accumulation of cortical flortaucipir signal (presumed accumulation of tau) whereas amyloid- $\beta$ - subjects did not. The magnitude of effect (about 2–3% per year relative to baseline SUVr) was remarkably similar despite the differences in method for SUVr calculation, duration of follow-up and differences in the subject populations (a longitudinal community sample versus a clinical trial sample). Both studies also reported an inverse relationship between age and baseline SUVr and a trend for younger subjects with higher baseline SUVr to also show greater longitudinal change.

However, this study also extends the Jack *et al.* (2018) study in two important ways. First, by stratifying the subjects into 'quartiles' on the basis of baseline SUVr values and evaluating change at a voxel level, we were able to see quartile-related (presumably disease severity-related) differences in focal flortaucipir accumulation that were probably averaged out in the Jack *et al.* (2018) analysis. Second, we not only examined the longitudinal change in flortaucipir PET signal, but we evaluated the relationship association of baseline flortaucipir SUVr, and change in flortaucipir SUVr with cognitive deterioration.

Both baseline and change from baseline in flortaucipir global (MUBADA/PERSI) SUVr were associated with

decrease in cognitive performance in amyloid- $\beta$ + subjects, even after correction for age, cognitive reserve (ANART), APOE4 carrier status and amyloid burden (florbetapir PET SUVr). Importantly, florbetapir SUVr was not retained in any of the models as a predictor of cognitive change as assessed by MMSE, ADAS or FAQ, consistent with the hypothesis that amyloid burden enables the spread of tau, but tau, rather than amyloid, is proximally related to neuronal dysfunction and associated cognitive impairment in Alzheimer's disease (Nelson *et al.*, 2007; Jack *et al.*, 2016; Pontecorvo *et al.*, 2017b).

Change in flortaucipir SUVr was strongly correlated with baseline flortaucipir SUVr, but the sample size was too small to confidently perform analyses to separate the effects of baseline and change in flortaucipir SUVr on cognitive performance. Baseline flortaucipir SUVr presumably represents the cumulative brain exposure to tau NFT at the time of the baseline scan, and will reflect both the neuronal damage that has accumulated during the course of the disease, as well as the regions where ongoing neurodegeneration is likely to impact cognition in the future. In contrast, change in flortaucipir SUVr reflects only spread of tau within the 18-month observation period, and some portion of this recently accumulated tau may not yet have had a significant impact on neuronal function. Additional studies (e.g. the ongoing confirmatory arm of the present study, NCT# 02016560) and a larger sample size are needed to determine the relative contributions of these factors. Such studies could help confirm whether there may be some delay between appearance of tau tangles and expression of neuronal damage in the form of cognitive deterioration as predicted by recent models of the progression of Alzheimer's disease (Jack *et al.*, 2013).

Taken together, these results provide longitudinal evidence that tau spread may follow the pattern predicted from cross-sectional autopsy studies. Moreover, these results suggest that the amount and location of tau (as evidenced by flortaucipir SUVr) at baseline may have implications both for the spread of tau and the cognitive deterioration that may occur over an 18-month period. These results suggest that it may be possible, even necessary, to use baseline tau as a selection or stratifying variable in clinical trials, instead of, or in addition to, currently used variables such as neuropsychological tests and amyloid status, thus reducing the expected variance in disease progression and cognitive change and improving the power to detect a therapeutic effect.

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## Competing interests

M.J.P., M.D.D. Sr, M.N., M.L., N.G., A.K.A., S.S., A.M., N.C.L., H.X., S.P.T., A.D.J., S.S., B.T., A.S.F. and M.A.M. are employees of Eli Lilly and Company and/or Avid Radiopharmaceuticals, and are minor shareholders of Eli Lilly and Company. S. Salloway receives research support and consultancy fees from Lilly, Biogen, Merck, Genentech, and Roche. He also receives research support from Avid, Novartis, and Functional Neuromodulation. P.M.D. received a grant (through his university) from Avid Radiopharmaceuticals and has received grants from and/or served as an advisor to several companies in this field. He is also a minor shareholder in several companies whose products are not discussed here and a co-inventor on patents which are not discussed here.

## Supplementary material

Supplementary material is available at *Brain* online.

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